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Assessment of diaphragmatic function through surface electromyography in healthy individuals. A cross-section observational study

Evaluación de la función diafragmática a través de electromiografía de superficie en personas sanas. Estudio observacional de corte transversal

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What do we know about this issue?

Surface electromyography (EMG) is a non-invasive and simple procedure with the potential for high sensitivity. It is painless and reduces the risk of invasive complications, thus promoting well-being, comfort, and costeffectiveness in the care of patients with respiratory disorders compared to other methods.

Reference values and data acquisition techniques, as well as the equipment used for this purpose, are not yet standardized or comparable among them.

¿Qué aporta este estudio de nuevo?

This study carries out an initial examination of diaphragmatic function using EMGs in healthy individuals, aiming to contribute to the standardization of methods and physiological values for this variable.

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Abstract

Introduction: Diaphragmatic surface electromyography is a procedure designed to assess the diaphragm. The physiological values of the electrical activity may have potential use in rehabilitation, sports training, ventilatory support withdrawal in critical care units and follow-up of respiratory disease.

Objective: To assess and describe the diaphragmatic function through surface electromyography in a population of individuals during spontaneous and forced breathing.

Methods: Observational, exploratory cross-sectional study including subjects with no comorbidities. Diaphragmatic surface EMG was performed measuring the mean quadratic root during tidal volume and vital capacity breathing. The body composition of the participants was also assessed.

Results: 28 males and 22 females were included in the study. The mean quadratic root of the tidal volume for two minutes was 13.94 μ V for females and 13.31 μ V for males. The vital capacity was 23.24 μ V for males and 22.4 μ V for females. A correlation was identified between the mean quadratic root, weight, and body surface.

Conclusions: Mean quadratic root values of tidal volume in two minutes in healthy females and males have been documented. The mean quadratic root values are correlated with the physiological and functional characteristics of the participants.

Keywords: Diaphragm; Electromyography; Surface electromyography; Anesthesiology; Anesthesia.

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Resumen

Introducción: La electromiografía de superficie diafragmática es un procedimiento para la evaluación diafragmática. Los valores fisiológicos de la actividad eléctrica tendrían aplicaciones potenciales en rehabilitación, entrenamiento deportivo, en el retiro ventilatorio en unidades de cuidado crítico y en el seguimiento a patologías respiratorias.

Objetivo: Evaluar y describir la función diafragmática a través de electromiografía de superficie diafragmática en una población de sujetos durante la respiración espontánea y la respiración forzada.

Métodos: Estudio observacional exploratorio de corte transversal en el que se incluyeron sujetos sin comorbilidades. Se realizó electromiografía de superficie diafragmática midiendo la raíz cuadrática media durante respiraciones de volumen corriente y capacidad vital. Adicionalmente, se valoró la composición corporal de los participantes.

Resultados: Se incluyeron 28 hombres y 22 mujeres. La raíz cuadrática media de volumen corriente por dos minutos fue de 13,94 µV para mujeres y 13,31 µV para hombres, mientras que la capacidad vital fue 23,24 µV para hombres y 22,4 µV para mujeres. Se encontró una correlación entre la raíz cuadrática media, el peso y la superficie corporal.

Conclusiones: Se han documentado los valores de la raíz cuadrática media de volumen corriente por dos minutos en mujeres y hombres sanos. Los valores de la raíz cuadrática media se correlacionan con características fisiológicas y funcionales de los participantes.

Palabras clave: Diafragma; Electromiografía; Electromiografía de superficie; Anestesiología; Anestesia.

INTRODUCTION

The diaphragm is the main inspiratory muscle (1,2) and it is involved in modulating the intraabdominal pressure, postural stability, cardiac function, lymph flow, labor, swallowing, and emesis; additionally, it provides a barrier against gastroesophageal reflux, among other physiological processes. (1) The assessment of this muscle is clinically important because several pathological conditions result in diaphragmatic weakness, paralysis and fatigue, that could be irreversible. (3) The most frequent alterations are diaphragmatic dysfunction, diaphragmatic paralysis, or structural changes such as congenital agenesis, congenital duplication, eventration, diaphragmatic hernia, inter alia. (3,4)

The assessment of the diaphragm may be conducted using invasive and noninvasive methods, and biological markers. (5-8) These methods may be helpful to predict respiratory function, as adjuvants when withdrawing mechanical ventilation, or in cardiopulmonary rehabilitation. Some of the most common methods are diaphragmatic excursion (8), estimating the transdiaphragmatic pressure with esophageal and gastric balloons (5), transdiaphragmatic ultrasound (9), and the measurement of skeletal troponin 1 (sTnl) (8); however, many of these methods are invasive, painful and observer-dependent.

In contrast, the diaphragmatic surface electromyography (EMG) is a simple, noninvasive, highly sensitive procedure (10), painless and reduces any potential invasive complications. If properly standardized, this approach could promote wellbeing, comfort and cost-effectiveness in patient care, as compared to other methods. However, there are no accurate data in healthy individuals, neither in patients with respiratory pathologies to establish reference values; moreover, the techniques to capture data and the equipment used are not yet comparable. (8,11) Among other design methodologies, there is a need to develop a baseline of physiological, exploratory and longitudinal studies, in different groups of individuals according to age, respiratory and physical conditions. The primary goal is to generate parameters that could provide the foundation for

future studies, particularly adapting the technique and adjusting the monitors to capture signals, as well as the parameters for procedures to filter cardiac electrophysiological signals. Consequently, this study is intended to do an initial exploration in healthy individuals. (12)

The purpose of the study was to assess and describe the diaphragmatic function using EMG in a healthy population between 18 to 40 years old, based on their physical characteristics such as age, gender, and a few anthropometric variables, in order to contribute to standardize the methods and the physiological values for this variable.

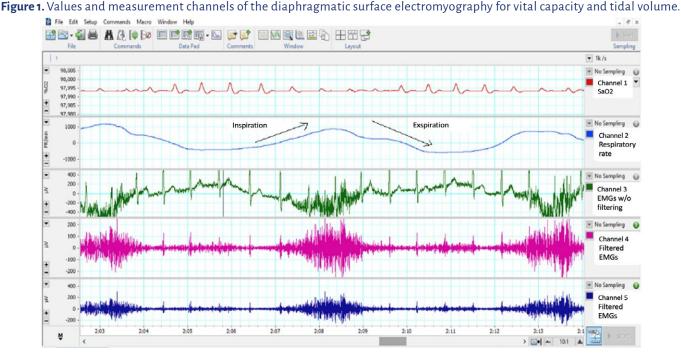
METHODS

An observational, exploratory, crosssectional study was conducted in individuals with no comorbidities, aged between 18 and 40 years. (4,13) The age range was selected taking into consideration the findings by various authors who identified that in average, sarcopenia starts to develop after 40 years of age. (4,14,15)

The sample included 50 individuals and it was estimated according to a formula of confidence intervals for medians based on the standard deviation derived from the study by Oliveira da Silva et al., who found a root mean square (RMS) SD = 17.88 μ V of the RMS (μ V) for healthy subjects in the Epidat 3.1 software. (16). Individuals with any contraindication for the EMG, with pacemakers or cardio defibrillator, with a history of recent surgeries or diaphragmatic lesions, who had received mechanical ventilation during the past 48 hours regardless of the modality, a history of corticosteroid use or muscle relaxants in the past two weeks, and individuals with underlying neurological, musculoskeletal, neuromuscular, respiratory and cardiovascular pathologies that could interfere with the results were excluded.

This project was assessed and approved by the ethics committee of Fundación Universitaria Navarra, minutes 007-1, of June 4, 2020, and all of the participants signed an informed consent before being admitted to the study. The measurement of electrical potentials resulting from muscle contraction was done with EMG (10). The motor unit action potentials were recorded, together with the frequency or pressure variations per unit of time (1 second) in the EMG signal which ranges between 2-500 Hz, in addition to amplitude variations, equivalent to energy changes of the signal generated during the passage of a wave which is around 2.1 microvolts (μ V) for large muscles, with a frequency of 500 Hz and a sensitivity signal amplitude of 500 μ V for the diaphragm and a frequency of 300 Hz and sensitivity signal amplitude of 300 μ V for other muscles, such as the abdominal muscles. (17-20) The electronic circuit measured was assessed in a portable computer to record the EMG, using the Power Lab® hardware and Labchart[®] software with the registered numbers shown in the RMS. (16)

The volunteers were asked to remain in supine position with a 35° head elevation and the leads arrangement was matrix/line ($3M^{\odot}$), two adhesive leads in the paraxiphoid region, 5 cm below de xiphoid process and other two in the costal margin region, bilateral, at a 16 cm distance (10). Posteriorly, the respiratory band was positioned approximately on the sixth intercostal space to record the ventilatory frequency and depth. Based on the equipment management protocol, the recording was initiated in 5 Labchart[®] channels (Figure 1): oxygen saturation was recorded in channel 1; respiratory movements in channel 2 the respiratory movements measured through the respiratory band -; the thoracic electrical signal was registered in channel 3, including the respiratory activity signals and cardiac activity; channel 4 was used for the first filtered tracing of the electrical activity of the diaphragm and respiratory muscles with a 1200 Hz Notch type filter; and channel 5 was used to filter channel 4 with a 500 Hz band filter. The signals were filtered so that the respiratory activity was the dominant activity for study purposes, minimizing the cardiac activity wave as much as possible, managing the high and low frequency sections expressed in Hz.



Channel 1: SaO2 of the participants. Channel 2: Recording of the respiratory band positioned in the chest. Channel 3: Electrical activity of the diaphragm, other respiratory muscles and the heart during three forced breathing cycles. Channel 4: The first tracing is the filtered electrical activity of the diaphragm and respiratory muscles with a 1200 Hz Notch type filter. Channel 5: Filter channel 4 with a 500 Hz band filter. **Source:** Authors.

Then the patient was instructed to breath normally for 2 minutes, in order to be able to record the tidal volume; then the patient was asked to take 3 forced inspirations and expirations (Figure 1).

Statistical analysis

The discrete or nominal variables were expressed in frequencies and proportions. Central tendency and scatter were used for the continuous variables and the Shapiro-Wilk for normality test was used to establish the behavior of the continuous variables. Correlation measures were taken (Spearman coefficient to determine the correlation of the relevant variables). The statistical test used to analyze the measurement differences was the Mann-Whitney U test, and for differences in proportion, the Fisher's test. A 5% level of significance was accepted for all the analyses (α = 0.05) and the differences were described together with 95% confidence intervals. The statistical analysis was conducted using the epi R software.

RESULTS

This study included 50 participants: 22 women (44 %) and 28 men (56 %), with a mean age of 23.3 years, (SD \pm 4.5) for females, and 27.1 years for males (SD \pm 6.4) (Table 1). The average weight for females was 59.3 kg (SD \pm 11.39), and for males 82.3 kg (SD \pm 16.1). The detailed characteristics of the participants are illustrated in Table 1.

The RSM for females was 13.94 μ V (SD ± 4.05 μ V). For males, the mean value obtained was 13.31 μ V (SD ± 5.48 μ V) (Table 2).

The RMS measurement during three consecutive breaths of vital capacity, resulted in higher values for males $-23.24 \,\mu$ V (SD \pm 8.58). Anthropometric variables were also compared, including height, weight and BMI, among other characteristics such as age and total body surface (TBS); with the RMS at VT, VC and R1, R2 and R3, a correlation was found between weight and RMS R1, and also with TBS (Table 3).

Table 1. General characteristics of the participants in the study (n = 50).

Variable	Females (n = 22) Mean <u>+</u> SD n (%)	Males (n = 28) Mean <u>+</u> SD n (%)
Age (years)	23.3 ± 4.5	27.1 <u>+</u> 6.4
Height (cm)	163 ± 5.4	174 ± 7.6
Weight (kg)	59.3 ± 11.3	82.3 <u>+</u> 16.1
Body surface (m2)	1.62 <u>+</u> 0.16	1.93 <u>+</u> 0.18
Body mass index (kg/m2)	22.2 <u>+</u> 4.1	27 ± 4
Low weight	3 (13)	1 (4)
Normal weight	16 (73)	7 (25)
Overweight	2 (9)	57.14 (16)
Obesity I	0	2 (7)
Obesity II	1 (5)	2 (7)
Physical exercise > 150 min/week	11 (50)	15 (54)
Physical exercise < 150 min/week	11 (50)	13 (46)

SD: standard deviation. **Source:** Authors.

Table 2. Root Mean Square Results (RMS) for tidal volume and vital capacity per 2 minutes.

Tidal volume	Females Males		
Mean µV (95 % CI)	13.94 (12.1-15.7)	13.31 (11.17-15.43)	
SD µV	4.05	5.48	
Ρ25 μV	9.92	10.22	
Ρ50 μV	15.28	13.29	
Ρ75 μV	17.14	16.11	
Ρ90 μV	17.57	19.27	
Ρ95 μV	18.99	24.65	
Vital capacity	Females	Males	
Mean μV (95 % CI)	22.4 (18.9-25.9)	23.24) (19.9-26.56)	
DS µV	7.9 8.58		
Ρ25 μV	16.73 16.53		
Ρ50 μV	20.51	22.52	
Ρ75 μV	28.23	8.23 28.47	
Ρ90 μV	35.34	33.73	
Ρ95 μV	37.61 41.5		

 μV : Microvolts; SD: Standard deviation. **Source:** Authors. Additionally, the BMI categories and the different RMS measurements were compared, and no relevant differences were identified. A stratification based on age and the RMS measurements for each range was performed, and 52 % of the sample was within an age range of 18 to 21 years. The highest RMS mean in VT breaths corresponds to the age range between 37 to 39 years (20.01 μ V). On the other hand, the lowest RMS VT value was found in the 27-30 year old group (6.52 μ V). In contrast, the lowest RMS VC value was found in the 30-33 year old group (19.95 μ V). In general for all age ranges, the RMS standard deviation did not show very scattered values, except for the 27-30 year old range (SD \pm 23.4).

DISCUSSION

This study assessed the diaphragmatic function using EMG to contribute to the RMS reference values in young adults 18 to 40 years old. Several body characteristics were also analyzed, including sex, age, TBS, BMI and physical condition. The EMG detected and analyzed the electrical activity of the diaphragm muscle associated with the contractile and motor activity – both voluntary and spontaneous. (21) **Table 3.** Correlation between the physical characteristics of the participants and RMS VT, RMS VC average and in R1, R2 and R3.

Variable	RMS VT	RMS CV	RMS R1	RMS R2	RMS R3
Age	Rho = 0.209 p	Rho =0.188	Rho =0.129	Rho =0.070 p	Rho = 0.109 p
	= 0.144	p =0.190	p =0.370	= 0.629	= 0.448
Height	R2 =0.141	Rho = 0.160 p	Rho = 0.224 p	Rho = 0.129 p	Rho = 0.160 p
	p =0.232 **	= 0.265	= 0.116	= 0.371	= 0.266
Weight	Rho = 0.129 p	R2 =0.246	Rho =0.298 p	Rho = 0.154 p	Rho = 0.181
	=0.369	p =0.084	=0.035	=0.284	p = 0.206
BMI	Rho =0.07	Rho =0.227	Rho =0.246 p	Rho = 0.113	Rho = 0.162 p
	p =0.585	p =0.112	=0.084	p = 0.430	= 0.258
TBS	Rho = 0.129 p	Rho =0.246 p	Rho = 0.298 p	Rho = 0.154 p	Rho = 0.181
	= 0.369	= 0.084	=0.035	= 0.284	p = 0.206



A few differences were found based on the body characteristics of the subjects studied, which were in some cases consistent with the available literature, and other cases were contradictory. Oliveira da Silva et al. (16) studied the differences in the electrical activity of the diaphragm in two groups (healthy individuals and patients with liver disease), including subjects with similar body weights and physical characteristics, with older ages than the subjects in this study. The RMS for healthy subjects was $49.39 \,\mu\text{V}$, (SD + 17.88), while for liver disease patients the RMS was 56.56 μ V (SD \pm 34.64); the latter could have sarcopenia, which develops after age 40, in addition to underlying conditions related to age, changes in the nutritional and metabolic status, which have an impact on the muscle dynamics. Oliveira da Silva et al. concluded that higher RMS values in patients with liver disease were associated with higher ventilatory effort (4,16,22); though they agreed that this instrument may be helpful as a tool in respiratory monitoring.

In this study the average RMS values were lower than those reported by Oliveira da Silva et al.: 22.4 μ V for females and 23.24 μ V for males; in VC ventilation, the highest mean RMS of VT and VC was for an age range between 37 to 39 years, but just 6% of the sample was within this range. Likewise, for the lowest RMS value in VT for the 27-

30 years age group, which represented 4 % of the study population. These conflicting results may be associated with differences in age and body composition of the participants in both trials. (16) However, Duarte et al. (10) found that the RMS values of the right and left diaphragm in spontaneous mode with minimal ventilation parameters, were $26.68 \pm 10.92 \mu$ V and $26.55 \pm 10.53 \mu$ V, respectively; and the RMS values after extubation were $31.93 \pm 18.69 \mu$ V to $34.62 \pm 13.55 \mu$ V, which is very similar to the findings in this study. (10)

Other studies such as Hawkes et al., examined healthy individuals and considered the effect of adding inspiratory load on the electrical activity of the diaphragm. (23) They found an increase in the RMS values during maximum inspiratory pressure, associated with the increased work of breathing during forced inspirations (maximum inspiratory pressure: 125.6 ± 30.8 cm H2O). The physical characteristics and the age of the subjects in the study by Hawkes et al. were similar to those included in this study, as well as the reported RMS values. (23). Moreover, other analyses such as Lokin et al. showed that the diaphragmatic EMG and the transesophageal EMG had a time correlation and concordance. With optimization of signal stability, diaphragmatic EMG may become a useful

respiratory monitoring tool, although there is a need for longitudinal studies of different populations to fine-tune the technique and reference values. (24,25) Currently there are clear guidelines for electromyography methods for various muscles (17); however, the respiratory muscle bundle remains a challenge due to its function and anatomical location.

This research project also explored some correlations with regards to the physical characteristics described as relevant by other authors; a correlation was identified between the TBS and higher RMS values; since 72.7 % of the female participants had an adequate BMI and 57.14 % of males were overweight, the RMS values were observed to be higher in individuals with a higher BMI. The is an increasing trend in the RMS values when the BMI is higher, which is consistent with the literature. (26-28) The study by Steier et al. used transesophageal electromyography with multipolar electrode and they reported that the higher the BMI, the work of breathing increases (27); this could be associated with thoracic changes in obese individuals which are reflected in increased elastic resistance, both of the lung and the chest wall, increasing the respiratory effort due to mechanical overload. Moreover, it was associated with a decrease in the pulmonary volumes affecting the inspiratory capacity, the expiratory reserve volume and VC. (28)

Additionally, some cases of fat infiltration in the respiratory muscles have been described, which are accompanied by muscle dysfunction, increased diaphragmatic electromyography activity, which does not necessarily involve increased inspiratory muscle pressure or insufficient muscle contraction. (28) According to Kelly et al., obesity decreases the chest compliance by up to 65%, because the excess adipose tissue in the chest and abdomen hinder the chest expansion. (29) Moreover, people with obesity as opposed to normal weight individuals, generate

higher VT inspiratory pressures to offset their poor respiratory performance which results in increased work of breathing; hence this population develops increased strength and capacity of the respiratory muscles. This may explain the increased RMS in overweight and obese individuals (29).

The RMS behavior with regards to gender showed no differences in this study. However, the measurements were taken at rest and some studies have found differences during physical activity. Molgat-Seon et al. found higher diaphragmatic RMS values in women and elderly adults during exercise. (30) Additionally, Mitchell et al. also assessed EMG of the diaphragm and extra-diaphragmatic inspiratory muscles during exercise and they identified gender differences and reported that extradiaphragmatic inspiratory muscles RMS was higher at all times during submaximal exercise in females. (31) They concluded that there may be a greater reliance on the extra-diaphragmatic inspiratory muscles in women relative to men. (31)

These sex differences were also reported by Guenette et al., who suggest that muscle fatigue in women may be lower because during exercise the load is distributed more uniformly over the respiratory muscles and there is also the involvement of the extra-diaphragmatic inspiratory muscles thus reducing the load on the diaphragm. This phenomenon has been associated with less muscle mass in women giving rise to the need to distribute the load on several respiratory muscles. (32,33). Moreover, Hawkes et al. (23) identified some sex differences, but these were not conclusive. (2,34)

The participants who exercised regularly >150 minutes per week, had lower VT RMS values as compared to those with a relatively sedentary lifestyle. This may be associated with overweight or decreased muscle mass since weight increase leads to higher respiratory effort; in contrast, physical activity has a favorable muscle effect. (3)

With regards to the value for monitoring the respiratory function, Hernández-Valdivieso et al. assessed the relationship between positive end-expiratory pressure (PEEP) on the respiratory muscle activity using EMG in individuals with noninvasive mechanical ventilation and obtained values associated with muscle work during inspiration and expiration. They concluded that EMG is quantitatively related to the PEEP level and the change in diaphragmatic and sternocleidomastoid activity. (11,20,35,36) This could be valuable in bedside monitoring of the critically ill patient; however, it is still necessary to further standardize the reference values and the specific signal filtering technique for these muscle groups in order to make them comparable between patients.

research contributes This with exploratory physiological data that may be the basis for further studies on a future instrument for bedside monitoring of the respiratory muscle function, once the above-mentioned challenges are overcome. The main limitations were the absence of complete spirometry measurements to correlate the EMG results with the RMS; additionally, no measurements were taken of the frequency domain of the electromyography waves and the sample was small. Moreover, there is a gap in our knowledge about the reference values for standardizing the diaphragmatic EMG amplitude during maximum voluntary isometric contractions and during moderate to intense physical activity. The findings in these young healthy subjects may not be generalized to other populations such as the elderly, critically ill patients or patients with respiratory failure.

CONCLUSIONS

The diaphragmatic function was assessed with the use of EMG in a population of healthy individuals, 18 to 40 years old. The tidal volume RMS for two minutes was 13.94 μ V in females and 13.31 μ V in males, while the vital capacity was 23.24 μ V for males and 22.4 μ V for females.

ETHICAL DISCLOSURES

Ethics committee approval

The study was approved by the Ethics Committee of Fundación Universitaria Navarra, minutes 007-1, of June 4, 2020

Protection of humans and animals

The authors declare that no experiments were conducted in humans or in animals for this research. The authors declare that the procedures followed were consistent with the ethical standards of the committee on responsible human experimentation and in accordance with the World Medical Association and the Declaration of Helsinki.

Confidentiality of the data

The authors declare that they have followed the protocols of their work place on the publication of data of patients or participating subjects.

Right to privacy and informed consent

The authors declare that this article does not disclose any patients' data. The authors have received the informed consent of all patients and/or subjects mentioned in the article. This document is in the possession of the corresponding author.

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Contribution by the authors

CYRT and CMSS: Study planning, data collection, interpretation of the results and drafting of the manuscript.

MEMP: Study planning, data collection, interpretation of the results, analysis of the data and drafting of the manuscript.

AMZ: Data collection, drafting of the manuscript.

Assistance for the study

None declared.

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Disclosures

The authors have no conflicts of interest to disclose

Presentations

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REFERENCES

- Kocjan J, Adamek M, Gzik-Zroska B, Czyżewski D, Rydel M. Network of breathing. Multifunctional role of the diaphragm: a review. Adv Respir Med. 2017;85(4):224-32. doi: <u>https://</u> doi.org/10.5603/ARM.2017.0037
- Aslan SC, McKay WB, Singh G, Ovechkin AV. Respiratory muscle activation patterns during maximum airway pressure efforts are different in women and men. Respir Physiol Neurobiol. 2019; 259:143-8. doi: <u>https://doi. org/10.1016/j.resp.2018.09.004</u>
- Ramsook AH, Molgat-Seon Y, Schaeffer MR, Wilkie SS, Camp PG, Reid WD, et al. Effects of inspiratory muscle training on respiratory

muscle electromyography and dyspnea during exercise in healthy men. J Appl Physiol Bethesda Md 1985. 2017;122(5):1267-75. doi: <u>ht-</u> tps://doi.org/10.1152/japplphysiol.00046.2017

- 4. Molina Peña ME, Sánchez CM, Rodríguez-Triviño CY. Physiopathological mechanisms of diaphragmatic dysfunction associated with mechanical ventilation. Rev Esp Anestesiol Reanim Engl Ed. 2020;67(4):195-203. doi: <u>https://doi.org/10.1016/j.redare.2019.12.003</u>
- Oppersma E, Hatam N, Doorduin J, van der Hoeven JG, Marx G, Goetzenich A, et al. Functional assessment of the diaphragm by speckle tracking ultrasound during inspiratory loading. J Appl Physiol. 2017;123(5):1063-70. doi: <u>https://doi.org/10.1152/japplphysiol.00095.2017</u>
- Hayat A, Khan A, Khalil A, Asghar A. Diaphragmatic excursion: Does it predict successful weaning from mechanical ventilation?. J Coll Physicians Surg—Pak. [Internet]. 2017;27(12):743-50. Available at: <u>https://pubmed.ncbi.nlm.nih.gov/29185398/</u>
- 7. Yoo JW, Lee SJ, Lee JD, Kim HC. Comparison of clinical utility between diaphragm excursion and thickening change using ultrasonography to predict extubation success. Korean J Intern Med. 2018;33(2):331-9. doi: <u>https://doi. org/10.3904/kjim.2016.152</u>
- Sánchez Sánchez CDM, Molina-Peña ME, Rodríguez-Triviño CY. Comprehensive assessment of respiratory function, a step towards early weaning from the ventilator. Adv Respir Med. 2021;89(3):299-310. doi: <u>https://doi.org/10.5603/ARM.a2021.0055</u>
- Ricoy J, Rodríguez-Núñez N, Álvarez-Dobaño JM, Toubes ME, Riveiro V, Valdés L. Diaphragmatic dysfunction. Pulmonology. 2019;25(4):223-35. doi: <u>https://doi.or-</u> g/10.1016/j.pulmoe.2018.10.008
- Duarte RP, Sentanin AC, da Silva AMO, Tonella RM, Duarte GL, Ratti LSR, et al. Diaphragm muscle surface electromyography in patients submitted to liver transplant and eligible for extubation. Transplant Proc. 2017;49(4):829-31. doi: <u>https://doi.org/10.1016/j.transproceed.2017.01.059</u>
- 11. Dos Reis IMM, Ohara DG, Januário LB, Basso-Vanelli RP, Oliveira AB, Jamami M. Surface electromyography in inspiratory muscles in adults and elderly individuals: A systematic review. J Electromyogr Kinesiol Off J Int Soc

Electrophysiol Kinesiol. 2019;44:139-55. doi: https://doi.org/10.1016/j.jelekin.2019.01.002

- 12. Kaufman MR, Elkwood AI, Colicchio AR, CeCe J, Jarrahy R, Willekes LJ, et al. Functional restoration of diaphragmatic paralysis: an evaluation of phrenic nerve reconstruction. Ann Thorac Surg. 2014;97(1):260-6. doi: <u>https://doi. org/10.1016/j.athoracsur.2013.09.052</u>
- 13. Elm E von, Altman DG, Egger M, Pocock SJ, Gøtzsche PC, Vandenbroucke JP. The Strengthening the Reporting of Observational Studies in Epidemiology (STROBE) statement: guidelines for reporting observational studies. J Clin Epidemiol. 2008;61(4):344-9. doi: https://doi.org/10.1016/j.jclinepi.2007.11.008
- Nedergaard A, Karsdal MA, Sun S, Henriksen K. Serological muscle loss biomarkers: an overview of current concepts and future possibilities. J Cachexia Sarcopenia Muscle. 2013;4(1):1-17. doi: <u>https://doi.org/10.1007/ s13539-012-0086-2</u>
- 15. Banus MS, Birchall MA, Graveston JA. Developing control algorithms of a voluntary cough for an artificial bioengineered larynx using surface electromyography of chest muscles: A prospective cohort study. Clin Otolaryngol Off J ENT-UK Off J Neth Soc Oto-Rhino-Laryngol Cervico-Facial Surg. 2018;43(2):562-6. doi: <u>https://doi.org/10.1111/coa.13022</u>
- 16. Oliveira da Silva AM, Maturi S, Boin IFSF. Comparison of surface electromyography in respiratory muscles of healthy and liver disease patients: preliminary studies. Transplant Proc. 2011;43(4):1325-6. doi: <u>https://doi.org/10.1016/j.transproceed.2011.03.058</u>
- Hermens HJ, Freriks B, Disselhorst-Klug C, Rau G. Development of recommendations for SEMG sensors and sensor placement procedures. J Electromyogr Kinesiol. 2000;10(5):361-74. doi: <u>https://doi.org/10.1016/S1050-</u> 6411(00)00027-4
- Gila Useros L, Malanda Trigueros A, Rodríguez Carreño I, Rodríguez Falces J, Navallas Irujo J. Electromyographic signal processing and analysis methods. 2009;32(Supp 3):27-43. doi: <u>https://doi.org/10.4321/S1137-66272009000600003</u>
- 19. Papagiannis GI, Triantafyllou AI, Roumpelakis IM, Zampeli F, Garyfallia Eleni P, Koulouvaris P, et al. Methodology of surface electromyography in gait analysis: review of the

literature.] Med Eng Technol. 2019;43(1):59-65. doi: <u>https://doi.org/10.1080/03091902.201</u> <u>9.1609610</u>

- 20. de Souza Costa HLL, de Souza LC, da Silva Neto AE, da Silva Guimarães BL, de Azeredo LM, Godoy MDP, et al. Involvement of respiratory muscles during the timed inspiratory effort index measurement with surface electromyography. Respir Care. 2020;65(12):1857-63. doi: <u>https://doi.org/10.4187/respcare.07465</u>
- 21. Dimitrova NA, Arabadzhiev TI, Hogrel JY, Dimitrov GV. Fatigue analysis of interference EMG signals obtained from biceps brachii during isometric voluntary contraction at various force levels. J Electromyogr Kinesiol Off J Int Soc Electrophysiol Kinesiol. 2009;19(2):252-8. doi: <u>https://doi.org/10.1016/j.jelekin.2007.08.007</u>
- Carvalho E, Isern M, Lima P, Machado C, Biagini A, Massarollo P. Força muscular e mortalidade na lista de espera de transplante de fígado. Rev Bras Fisioter. 2008;12(3):235-40. doi: <u>https://doi.org/10.1590/S1413-35552008000300012</u>
- 23. Hawkes EZ, Nowicky AV, McConnell AK. Diaphragm and intercostal surface EMG and muscle performance after acute inspiratory muscle loading. Respir Physiol Neurobiol. 2007;155(3):213-9. doi: <u>https://doi.org/10.1016/j.resp.2006.06.002</u>
- 24. Lokin JL, Dulger S, Glas GJ, Horn J. Transesophageal versus surface electromyography of the diaphragm in ventilated subjects. Respir Care. 2020;65(9):1309-14. doi: <u>https://doi.</u> <u>org/10.4187/respcare.07094</u>

- 25. Zhang DD, Lu G, Zhu XF, Zhang LL, Gao J, Shi LC, et al. Neural respiratory drive measured using surface electromyography of diaphragm as a physiological biomarker to predict hospitalization of acute exacerbation of chronic obstructive pulmonary disease patients. Chin Med J (Engl). 2018;131(23):2800-7.
- 26. Bailey CA, Corona F, Pilloni G, Porta M, Fastame MC, Hitchcott PK, et al. Sex-dependent and sex-independent muscle activation patterns in adult gait as a function of age. Exp Gerontol. 2018;110:1-8. doi: <u>https://doi.org/10.1016/j.exger.2018.05.005</u>
- 27. Steier J, Jolley CJ, Seymour J, Roughton M, Polkey MI, Moxham J. Neural respiratory drive in obesity. Thorax. 2009;64(8):719-25. doi: <u>ht-</u> <u>tps://doi.org/10.1136/thx.2008.109728</u>
- Dixon AE, Peters U. The effect of obesity on lung function. Expert Rev Respir Med. 2018;12(9):755-67. doi: <u>https://doi.org/10.1080</u> /17476348.2018.1506331
- 29. Kelly TM, Jensen RL, Elliott CG, Crapo RO. Maximum respiratory pressures in morbidly obese subjects. Respir Int Rev Thorac Dis. 1988;54(2):73-7. doi: <u>https://doi.</u> org/10.1159/000195504
- 30. Molgat-Seon Y, Dominelli PB, Ramsook AH, Schaeffer MR, Romer LM, Road JD, et al. Effects of age and sex on inspiratory muscle activation patterns during exercise. Med Sci Sports Exerc. 2018;50(9):1882-91. doi: <u>https://</u> doi.org/10.1249/MSS.000000000001648
- 31. Mitchell RA, Schaeffer MR, Ramsook AH, Wilkie SS, Guenette JA. Sex differences in respiratory muscle activation patterns during

high-intensity exercise in healthy humans. Respir Physiol Neurobiol. 2018;247:57-60. doi: https://doi.org/10.1016/j.resp.2017.09.002

- 32. Guenette JA, Romer LM, Querido JS, Chua R, Eves ND, Road JD, et al. Sex differences in exercise-induced diaphragmatic fatigue in endurance-trained athletes. J Appl Physiol Bethesda Md 1985 2010;109(1):35-46. doi: https://doi.org/10.1164/ajrccm-conference.2010.181.1_MeetingAbstracts.A5319
- 33. Geary CM, Welch JF, McDonald MR, Peters CM, Leahy MG, Reinhard PA, et al. Diaphragm fatigue and inspiratory muscle metaboreflex in men and women matched for absolute diaphragmatic work during pressure-threshold loading. J Physiol. 2019;597(18):4797-808. doi: https://doi.org/10.1113/JP278380
- 34. Mauvais-Jarvis F. Sex differences in metabolic homeostasis, diabetes, and obesity. Biol Sex Differ. 2015;6:14. doi: <u>https://doi.org/10.1186/</u> <u>s13293-015-0033-y</u>
- 35. Hernández-Valdivieso AM, Salazar-Sánchez MB, Muñoz-Ortega IC. Efecto del incremento de la PEEP en la actividad muscular respiratoria evaluado con electromiografía de superficie en individuos sanos bajo ventilación espontánea. latreia. 2016;29(3):280-91. doi: <u>https://doi. org/10.17533/udea.iatreia.v29n3a03</u>
- 36. Ajiro Y, Shiga T, Shoda M, Hagiwara N. Surface electromyography of myopotential oversensing provoked by simultaneous straining and leftward twisting in a patient with an implantable cardioverter defibrillator. Heart Vessels. 2017;32(3):364-8. doi: <u>https://doi. org/10.1007/s00380-016-0888-9</u>