

## ORIGINAL RESEARCH

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# Variations in glenohumeral movement control when implementing an auditory feedback system: A pilot study

*Variaciones en el control del movimiento glenohumeral al implementar un sistema de retroalimentación auditiva: un estudio piloto*

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## | Abstract |

**Introduction:** Human motor control requires a learning process and it can be trained by means of various sensory feedback sources.

**Objective:** To determine variations in glenohumeral movement control by learning in young adults exposed to an auditory feedback system while they perform object translation tasks classified by difficulty level.

**Materials and methods:** The study involved 45 volunteers of both sexes (22 women), aged between 18 and 32 years. Glenohumeral movement control was measured by means of the root mean square (RMS) of the accelerometry signal, while task execution speed (TES) was measured using an accelerometer during the execution of the task according to its difficulty (easy, moderate and hard) in four stages of randomized intervention (control, pre-exposure, exposure-with auditory feedback, and post-exposure).

**Results:** Statistically significant differences ( $p < 0.001$ ) were found between the pre-exposure and exposure stages and between pre-exposure and post-exposure stages. A significant increase ( $p < 0.001$ ) in TES was identified between the pre-exposure and exposure stages for tasks classified as easy and hard, respectively.

**Conclusion:** The use of an auditory feedback system in young adults without pathologies enhanced learning and glenohumeral movement control without reducing TES. This effect was maintained after the feedback, so the use of this type of feedback system in healthy individuals could result in a useful strategy for the training of motor control of the shoulder.

**Keywords:** Motor Activity; Feedback, Sensory; Psychomotor Performance (MeSH).

## | Resumen |

**Introducción.** El control del movimiento humano requiere de un proceso de aprendizaje y puede ser entrenado por medio de la retroalimentación proveniente de diversas fuentes sensoriales.

**Objetivo.** Determinar variaciones en el control del movimiento glenohumeral por aprendizaje en adultos jóvenes sometidos a un sistema de retroalimentación auditiva, mientras realizan tareas de traslación de objetos clasificadas por nivel de dificultad.

**Materiales y métodos.** Participaron 45 voluntarios de ambos sexos (22 mujeres) entre 18 y 32 años. El control del movimiento glenohumeral se midió por medio de la raíz media cuadrática de acelerometría, mientras que para la velocidad de ejecución de la tarea (VE) se usó un acelerómetro durante la ejecución de tareas según dificultad (fácil, moderado y difícil) en cuatro etapas aleatorizadas de intervención (control, pre-exposición, exposición con retroalimentación auditiva y post-exposición).

**Resultados.** Se encontraron diferencias significativas ( $p < 0.001$ ) entre las etapas pre-exposición y exposición, y entre pre-exposición y post-exposición. Se identificó un aumento significativo de la VE entre pre-exposición y exposición para tareas con clasificación fácil y difícil.

**Conclusión.** El uso de un sistema de retroalimentación auditiva en adultos jóvenes sin patologías podría favorecer el aprendizaje y el control del movimiento glenohumeral sin disminuir la VE, resultado que se mantiene luego de la retroalimentación, por lo que el uso de un sistema de retroalimentación auditiva en individuos sanos podría resultar en una estrategia útil para el entrenamiento del control motriz del hombro.

**Palabras clave:** Actividad motora; Retroalimentación sensorial; Desempeño psicomotor (DeCS).

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## Introduction

Motor learning is a key adaptive mechanism for solving problems of daily life that is used to maintain known behavioral capacities and to learn new skills. (1) Human motor control requires a learning and training process known as feedback, in which the nervous system makes a constant comparison between the desired value and the value it receives in real time from the environment. (2-4)

Hence, the use of a system that feeds back in a positive or negative way the execution of a motor gesture could modulate this movement, which would favor learning. (1-5) In this sense, there is a series of techniques and tools that provide feedback on the movement performed and influence its control. (3,6) These tools, used both in physical rehabilitation and in sports training, are associated mainly to visual, tactile, proprioceptive and auditory stimuli; the latter has not been studied sufficiently. (3)

Rosati *et al.* (5) used visual and auditory feedback together, and demonstrated that they would help improve performance and learning in the execution of exercises with the upper limbs. On the other hand, Portnoy *et al.* (7) demonstrated the effectiveness of auditory feedback compared to kinesthetic learning during the execution of a motor gesture, a result that has not been reported in other studies focused on learning the movement generated with this type of intervention.

Furthermore, an objective evaluation to measure motor control of the upper limb and, specifically, of glenohumeral movement requires sophisticated systems that, in general, are inefficient for clinical

practice, since they are time-consuming, costly and may require a laboratory. (8) Therefore, several studies (8-15) highlight the benefits of accelerometers and inertial sensors as inexpensive and easy to use methods that provide reliable and fast data.

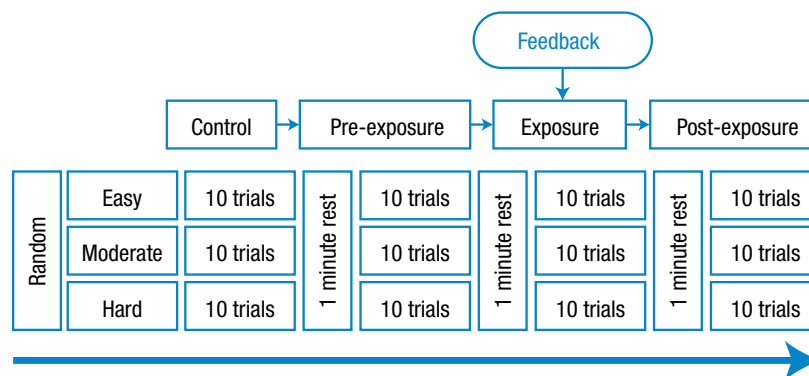
Root mean square (RMS) is a measure of central tendency (16) that is used in various studies to measure the vibration of different segments of the human body in the context of motion analysis. (13,14,17,18) Similarly, Körver *et al.* (8) have proposed to study clinical shoulder variables with accelerometry and to include acromion-sensor distance (ASD), body mass index (BMI) and sex within the analyses.

With this in mind, the objective of this research is to determine variations in glenohumeral movement control through learning in young adults exposed to an auditory feedback system, while performing object translation tasks classified by difficulty level.

## Materials and methods

### Design

Cross-sectional study with time series evaluations including four measurement stages in the same group: control, pre-exposure, exposure (with auditory feedback) and post-exposure. Figure 1 presents the four stages of the research, which consisted of the tasks that were executed, classified according to the difficulty level. The third stage (exposure) corresponds to that implemented with the auditory feedback system.



**Figure 1.** Research design. Source: Own elaboration.

### Participants

The sample consisted of 45 young adults (22.78+3.45 years) of both sexes (23 men and 22 women) with a BMI of 27.30+5.31 and an ASD of 29.86+2.07cm. The participants, who came from the Araucanía region of Chile, agreed to participate freely in the study by signing an informed consent form and were selected in a non-probabilistic, intentional manner. Sample size was determined using the method proposed by Hulley *et al.* (19)

The inclusion criteria were: being a university student over 18 years of age and having access to the evaluation during the period of execution (six months) as planned. The exclusion criteria were: having a history of painful shoulder conditions, having a pathology directly or indirectly associated with the function of the upper limb, and having

hearing impairment or sensory processing disorders. In order to confirm the suitability for the study, each participant took a brief recognition test of the musical notes that would be used in the feedback, during which they were requested to classify the notes as low-pitched or high-pitched; an error of 20% was considered an exclusion criterion.

The measurement protocol was approved by the Institutional Ethics Committee of the Universidad de Santiago de Chile through Minutes No. 576 of October 17, 2016 and was developed in accordance with the ethical principles of the Declaration of Helsinki. (20)

### Measurements

During the pilot study, an auditory feedback system based on accelerometry was implemented, since these types of sensors are

widely used in various electronic devices, which would favor transfer and massification.

The sensor used was an analog accelerometer (Freescale Semiconductor® model MMA7361, USA) that was connected to an electronic board (Arduino® model UNO, Italy), and communicated to a laptop computer (ASUS model X455L, China) via a serial port; the data was collected using Matlab® software, version R2012b (USA). The acceleration sensor was adhered to the skin with double-sided tape at the midpoint of the triangle formed by the olecranon, lateral epicondyle and medial epicondyle of the humerus while the elbow was in 90° flexion. (8,9,21)

Accelerometer measurement data were obtained throughout four consecutive study stages. Based on previous research (15), a protocol adapted to the objective of the study was planned, including 10 trials for each difficulty level of the task, divided into blocks of 40 seconds with a pause of 1 minute, totaling 120 trials per participant.

In order to obtain the accelerometry RMS and the task execution speed (TES), the digitized raw data were processed. Firstly, the data were processed using a 4<sup>th</sup>-order Butterworth low pass digital filter with a cutoff frequency of 10Hz. Secondly, to eliminate the effects of the sensor position, the signal was centered at zero and a copy of it, softened with the same type of filter, was subtracted with a cutoff frequency of 0.1Hz. (22) Then, the RMS was calculated for the resulting signal and, finally, it was multiplied by the force of gravity and the acceleration obtained in velocity was integrated.

## Intervention

The intervention consisted of four stages which were distributed as follows:

*Control:* The participants were explained that the vibration or position of their arm during movement was going to be measured. To this end, they were asked to perform the easy, moderate and hard tasks.

*Pre-exposure:* The procedure carried out in the control stage was repeated.

*Exposure (with auditory feedback):* Participants were told that the vibrations or position of their arm during movement was going to

be measured while listening to a musical note (A, B, C, D, E, F and G). The musical note emitted, which depends on the vibration or position of the arm, would be high-pitched at higher vibration and low-pitched at lower vibration, so the instruction was to perform the tasks by making the system play low-pitched notes.

*Post-exposure:* The procedure carried out in the control stage was repeated.

In order to classify the tasks performed in each of the stages according to difficulty, the Flexilevel Scale of Shoulder Function was adapted taking into account the materials available in the evaluation laboratory. This scale consists of three subsets of items (tasks) that allow the general classification of different levels of shoulder function. (23) In this way, the tasks were classified as:

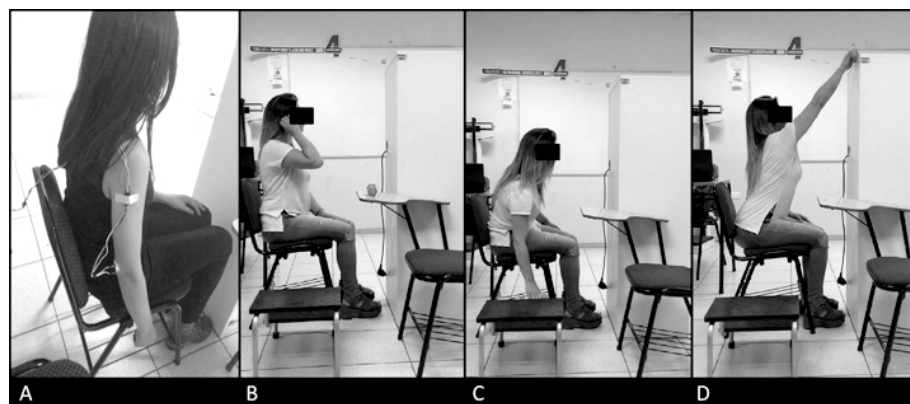
*Easy:* The participants were seated and had to touch the earlobe of the same side of their dominant arm, and then return to the initial position.

*Moderate:* The participants were seated and required to move a 2kg dumbbell from a 19cm high footstool with the dominant arm, located 5cm from their side, to a 70cm table located 17cm in front of them, and then return to the initial position.

*Hard:* The participants were seated and required to move a 2kg dumbbell with the dominant arm from a table located 22cm in front of them to a 142cm shelf and then return to the initial position.

## Procedure

Each volunteer was assigned a date and time for the measurements. First, a brief interview was conducted to collect information on age, sex, and upper limb dominance. Then, body weight and height of the feet were obtained to calculate the BMI (24) by means of a mechanical patient weighing scale with a measuring rod (Detecto® model 339, USA; accuracy 0.1kg and 0.1cm). The accelerometer was then placed and the ASD was measured using the Sanny anthropometric tape (Brazil; accuracy 0.1cm) from the lateral border of the acromion to the midpoint of the sensor. (8,9) Finally, the evaluation was carried out using an accelerometer-based system, in four successive stages, where the order of the difficulty level was random (Figure 2).



**Figure 2.** Execution of the tasks with different difficulty levels. A) initial position of the participants and positioning of the inertial sensor; B) easy task; C) moderate task; D) hard task.

Source: Own elaboration.

## Statistical analysis

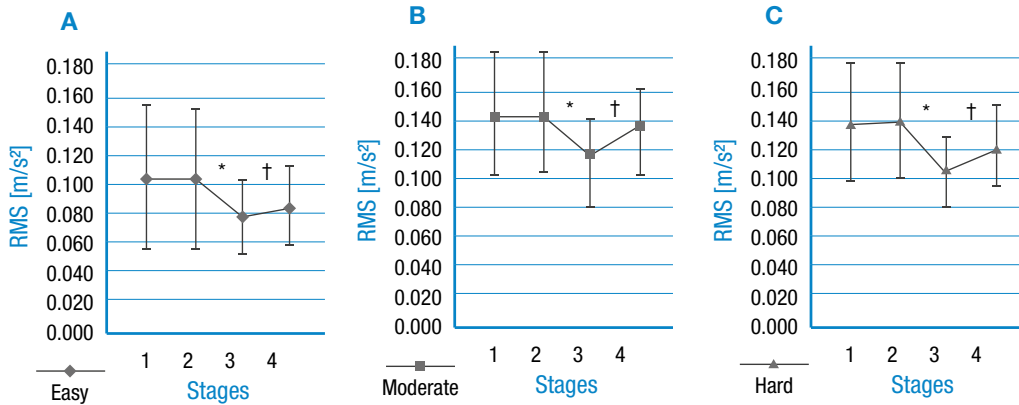
The Statistical Package for the Social Sciences® (SPSS) version 23.0 was used for analysis. The data were subjected to the Shapiro-Wilk normality test. The Wilcoxon nonparametric test was used to identify differences in the means of the dependent variables; the Spearman

ranges test was used to establish correlations according to the different tasks and stages of the study (between the variables RMS and TES; RMS and ASD; RMS and BMI); the point-biserial correlation was used for nonparametric correlation analysis of independent variables to determine the correlation between RMS and sex. In all cases, a significance level of  $p < 0.05$  was established.

### Results

A significant decrease in RMS was observed during the exposure stage (Figure 3). Statistically significant differences were found between

the pre-exposure and exposure stages ( $p < 0.001$ ), and between pre-exposure and post-exposure for the three task difficulty levels (Table 1). Statistically significant differences were compared using the Wilcoxon test. Data were expressed in mean and standard deviation.



**Figure 3.** Root Mean Square (mean) of the participants ( $n=45$ ) according to the stage and difficulty of the task. A) trials associated with an easy task; B) trials associated with a task of moderate difficulty; C) trials associated with a hard task. 1: control stage; 2: pre-exposure stage; 3: exposure stage; 4: post-exposure stage.

\* represents statistically significant differences ( $p < 0.01$ ) between the pre-exposure and exposure stages.  
 † represents statistically significant differences ( $p < 0.01$ ) between the pre-exposure and post-exposure stages.  
 Source: Own elaboration.

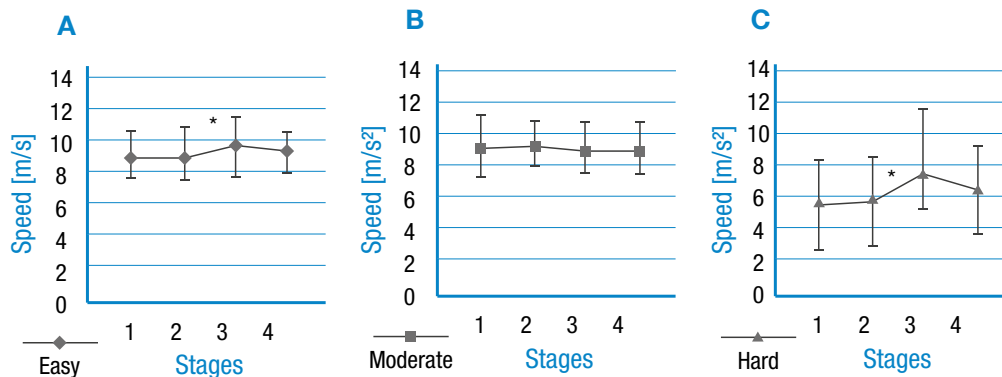
**Table 1.** Differences (mean) of the root mean square and the speed of execution of the task between the stages of the study and difficulty level of the task.

(n=45)		Control vs. pre-exposure. Mean ( $\sigma$ )	Pre-exposure vs. exposure. Mean ( $\sigma$ )	Pre-exposure vs. post-exposure. Mean ( $\sigma$ )
Easy	RMS ( $m/s^2$ )	0.103(0.05) vs. 0.102(0.05)	0.102(0.05) vs. 0.075(0.03) *	0.102(0.05) vs. 0.085(0.03) *
	TES (m/s)	8.99(1.44) vs. 8.91(1.72)	8.91(1.72) vs. 9.61(1.89) *	8.91(1.72) vs. 9.27(1.26)
Moderate	RMS ( $m/s^2$ )	0.143(0.04) vs. 0.145(0.04)	0.145(0.04) vs. 0.111(0.03) *	0.145(0.04) vs. 0.134(0.03) †
	TES (m/s)	9.28(1.88) vs. 9.38(1.47)	9.38(1.47) vs. 9.11(1.63)	9.38(1.47) vs. 9.10(1.63)
Hard	RMS ( $m/s^2$ )	0.136(0.04) vs. 0.138(0.04)	0.138(0.04) vs. 0.106(0.02) *	0.138(0.04) vs. 0.121(0.03) *
	TES (m/s)	5.48(2.79) vs. 5.74(2.87)	5.74(2.87) vs. 7.22(2.39) *	5.74(2.87) vs. 6.35(2.76)

$\sigma$ : standard deviation; RMS: raíz root mean square; TES: task execution speed.  
 \*  $p < 0.001$   
 †  $p < 0.01$   
 Source: Own elaboration.

Regarding TES, a significant increase ( $p < 0.001$ ) in speed between the pre-exposure and exposure stages was identified for tasks classified

as easy and hard (Figure 4). Statistically significant differences were compared using the Wilcoxon test.



**Figure 4.** Average execution speed of the participants ( $n=45$ ) depending on the stage and difficulty of the task. A) trials associated with an easy task; B) trials associated with a task of moderate difficulty; C) trials associated with a difficult task. 1: control stage; 2: pre-exposure stage; 3: exposure stage; 4: post-exposure stage.

\* represents statistically significant differences ( $p < 0.01$ ) between the pre-exposure and exposure stages.  
 Source: Own elaboration.

By correlating the RMS with its corresponding TES for each stage and task difficulty, it was found that in the post-exposure stage of the easy task there was a slightly significant inverse correlation ( $p=0.047$ ), which also has a very small coefficient ( $r=-0.298$ ), while the pre-exposure and exposure stages do not have statistically significant differences (Table 2). An inverse correlation between RMS and ASD was found in all the task difficulties and

at all stages. A direct correlation between the RMS and BMI variables was observed in the control, pre-exposure and post-exposure stages for the easy and moderate tasks. In addition, an inverse correlation between RMS and sex was reported for all task and stage difficulties (Table 2). For the correlation between RMS and sex, point biserial correlation coefficient was used, where 0=female and 1=male.

**Table 2.** Correlations between the variables of the study, distributed by stage and difficulty level of the task.

(n=45)		Control (valor r)	Pre-exposure (r-value)	Exposure (r-value)	Post-exposure (r-value)
Easy	RMS - TES	-0.071	0.075	-0.083	-0.298*
	RMS - ASD	-0.317*	-0.396 †	-0.378 †	-0.279
	RMS - Sex	-0.452 ‡	-0.441 †	-0.616 ‡	-0.505 ‡
	RMS - BMI	0.375*	0.438 †	0.333	0.521 †
Moderate	RMS - TES	0.156	-0.087	-0.042	0.117
	RMS - ASD	-0.482 ‡	-0.495 ‡	-0.404 †	-0.312*
	RMS - Sex	-0.500 ‡	-0.408 †	-0.529 ‡	-0.451 †
	RMS - BMI	0.415*	0.420*	0.304	0.478 †
Hard	RMS - TES	-0.145	-0.270	-0.094	-0.275
	RMS - ASD	-0.440 †	-0.478 ‡	-0.465 ‡	-0.363*
	RMS - Sex	-0.549 ‡	-0.553 ‡	-0.645 ‡	-0.594 ‡
	RMS - BMI	0.147	0.151	0.066	0.143

RMS: root mean square; TES: task execution speed; ASD: acromion-sensor distance; BMI: body mass index; r-value: correlation coefficient through Spearman rank correlation.

\*  $p<0.05$

†  $p<0.01$

‡  $p<0.001$

Source: Own elaboration.

## Discussion

The most relevant result of this research points to the existence of variations in the control of glenohumeral movement when implementing an auditory feedback system, which are manifested at all difficulty levels of the task.

Huang *et al.* (15) report a direct correlation between the difficulty of a range task and the magnitude of the accelerometry signal vector. In this respect, our results indicate a higher RMS of accelerometry in the task of moderate difficulty, followed by the hard and the easy tasks, in that order. The task of moderate difficulty presented a greater tendency to leave the sagittal plane while the movement was being executed, which could have a direct impact on the RMS obtained. However, this variation could be the result of several factors such as the number of participants, so it would be advisable to expand the sample to find if the trend persists.

When comparing the RMS between the pre-exposure and exposure stages, statistically significant differences were found in the three task difficulties, so the intervention would be favorable for decreasing the RMS. This is interpreted as a better control of the glenohumeral movement due to a lower number of adjustments during performance. On the contrary, no significant differences were reported between the control and pre-exposure stages for RMS and TES, which would indicate that the execution of 10 trials in these stages does not modify the execution of the movement in the participants.

When evaluating the RMS between the pre-exposure and post-exposure stages, statistically significant differences were found in the three task difficulties; therefore, the intervention continues to produce variations in the post-exposure stage. This could be associated with a

modification of the motor strategy after receiving auditory feedback (3), i.e., the intervention would contribute to motor learning in the participants.

With respect to TES, statistically significant differences were found in the easy and hard tasks with a tendency towards an increase in speed. In this regard, Sugamoto *et al.* (25) state that rapid movements represent better the motor functionality of humans, as the speed of the movement determines the motor strategy used. Consequently, the findings of this study become useful information for future research on the subject, since the intervention would not slow down the movement.

An attempt was made to identify a possible correlation between RMS and TES, since a correlation between repetitive TES and muscle response was previously found (26); it could be assumed that a task performed at low speed is related to lower values of RMS. The results of this research showed that RMS decreases without the need for a slower execution of the task, which could indicate that the feedback used generates a better response in the participants.

In relation to the covariates analyzed, studies with similar evaluation procedures (8,9) identified ASD as a possible modifier of the accelerometry signal, which coincides with the results of this research, since RMS had an inverse correlation ( $p<0.05$ ) with ASD. There was a lower RMS in the participants who had short humerus, a result that could indicate that the amplitude of the accelerometry signal decreases the closer the sensor is to the axis of motion. (8,9)

The RMS correlated directly with the female sex, which would indicate a greater number of accommodations with respect to the trajectory of movement. Likewise, having a high BMI correlated with greater adjustment in men and women, a fact that could be linked to

the physical-functional capacity of the participants. Although sex and BMI were related to RMS, no studies with similar characteristics were found to compare the results, so these variables should be addressed in future interventions.

The use of an objective measurement of low cost through accelerometers is one of the strengths of this study, since these sensors are found in most smartphones (27), thus turning into an opportunity to apply auditory feedback or other similar tools in these devices. Other elements that favor the internal validity of the measurements are the low difference obtained between the control and pre-exposure stages, the scarce time elapsed between the tasks, and their random order of execution.

One of the limitations was that the sensor used does not have the best quality in the market, which leads to a higher noise level; however, the used offline digital filtering processes helped to obtain the produced signal. Likewise, the weight of the transferred object according to the physical characteristics of the participants or sex was not considered. With all this in mind and considering the sample size, it is not possible to generalize the results of the study. However, new research could compare the results with a larger group of participants with different age ranges or even with a motor deficit.

In a practical context, this auditory feedback system is useful as a teaching-learning strategy for the control of glenohumeral movement during object translation tasks, which would support its use as a tool to choose exercises for the rehabilitation of function in the upper limbs. Another application that could result from this research is the use of auditory feedback as an intermediate stage between visual feedback and proprioceptive feedback, or it could even be used as a rehabilitation tool for people with visuomotor impairments and visual impairment. However, more research is needed in this field for its clinical application.

## Conclusion

The use of an auditory feedback system in young adults without pathologies could favor learning and control of glenohumeral movement without reducing TES. This effect is maintained after feedback, so the use of this type of feedback system in healthy individuals could result in a useful strategy for the training of motor control of the shoulder.

## Conflicts of interest

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## References

1. **Lalazar H, Vaadia E.** Neural basis of sensorimotor learning: modifying internal models. *Curr Opin Neurobiol.* 2008;18(6):573-81. <http://doi.org/d3472d>.
2. **Vogt K, Pirrò D, Kobenz I, Hölzlrich R, Eckel G.** PhysioSonic - Evaluated movement sonification as auditory feedback in physiotherapy. In: International Conference on Auditory Display. Copenhagen: Springer, Berlin, Heidelberg; 2009. 103-20.
3. **Boyer EO, Colin-Malagon L, Bevilacqua F, Susini P, Hannelton S.** Continuous sound feedback in tracking tasks. In: Multisensory Motor Behavior: Impact of Sound. Hannover: Leibniz Universität Hannover; 2013.
4. **Shea CH, Wulf G.** Enhancing motor learning through external-focus instructions and feedback. *Hum Mov Sci.* 1999;18(4):553-71. <http://doi.org/ftmjrc>.
5. **Rosati G, Oscari F, Spagnol S, Avanzini F, Masiero S.** Effect of task-related continuous auditory feedback during learning of tracking motion exercises. *J Neuroeng Rehabil.* 2012;9:79. <http://doi.org/c385>.
6. **Boyer EO, Babayan BM, Bevilacqua F, Noisternig M, Warusfel O, Roby-Brami A, et al.** From ear to hand: the role of the auditory-motor loop in pointing to an auditory source. *Front Comput Neurosci.* 2013;7:26. <http://doi.org/c386>.
7. **Portnoy S, Halaby O, Dekel-Chen D, Dierick F.** Effect of an auditory feedback substitution, tactilo-kinesthetic, or visual feedback on kinematics of pouring water from kettle into cup. *Appl Ergon.* 2015;51:44-9. <http://doi.org/c387>.
8. **Körver RJ, Senden R, Heyligers IC, Grimm B.** Objective outcome evaluation using inertial sensors in subacromial impingement syndrome: a five-year follow-up study. *Physiol Meas.* 2014;35(4):677-86. <http://doi.org/c388>.
9. **Körver RJ, Heyligers IC, Samijo SK, Grimm B.** Inertia based functional scoring of the shoulder in clinical practice. *Physiol Meas.* 2014;35(2):167-76. <http://doi.org/c389>.
10. **Godfrey A, Conway R, Meagher D, ÓLaighin G.** Direct measurement of human movement by accelerometry. *Med Eng Phys.* 2008;30(10):1364-86. <http://doi.org/ffd33d>.
11. **Hurd WJ, Morrow MM, Miller EJ, Adams RA, Sperling JW, Kaufman KR.** Novel approaches to objectively assess shoulder function. *J Shoulder Elbow Surg.* 2014;23(10):251-5. <http://doi.org/f2t8ft>.
12. **Cope E.** Estimating Human Movement Using a Three Axis Accelerometer. A Qualifying Examination Presented in Partial Fulfillment of the Requirements for the Degree Doctor of Philosophy [tesis doctoral]. Arizona: Arizona State University; 2009.
13. **Dahlqvist C, Hansson GÅ, Forsman M.** Validity of a small low-cost triaxial accelerometer with integrated logger for uncomplicated measurements of postures and movements of head, upper back and upper arms. *Appl Ergon.* 2016;55:108-16. <http://doi.org/f3vg98>.
14. **Lindsay TR, Yaggie JA, McGregor SJ.** A wireless accelerometer node for reliable and valid measurement of lumbar accelerations during treadmill running. *Sports Biomech.* 2016;15(1):11-22. <http://doi.org/c39b>.
15. **Huang HY, Chen WC, Cheng WC, Lai YT, Lin JJ.** RT3 accelerometer shoulder activity: discrimination of activity levels by the RT3 accelerometer for the assessment of shoulder physical activity (SPA). *Man Ther.* 2011;16(2):172-6. <http://doi.org/bjv69p>.
16. **Mitacc-Meza M.** *Temas de estadística descriptiva y probabilidad.* Lima: Thales; 1996.
17. **Tanoue H, Mitsuhashi T, Sako S, Goto R, Nakai T, Inaba R.** Effects of a dynamic chair on pelvic mobility, fatigue, and work efficiency during work performed while sitting: a comparison of dynamic sitting and static sitting. *J Phys Ther Sci.* 2016;28(6):1759-63. <http://doi.org/c39c>.
18. **Schütte KH, Aeles J, De Beéck TO, Van der Zwaard BC, Venter R, Vanwanseele B.** Surface effects on dynamic stability and loading during outdoor running using wireless trunk accelerometry. *Gait Posture.* 2016;48:220-5. <http://doi.org/f8xrnn>.
19. **Hulley SB, Cummings SR, Browner WS, Grady DG, Newman TB.** *Designing Clinical Research.* 3<sup>rd</sup> ed. Filadelfia: Lippincott, Williams & Wilkins; 2007.
20. Asociación Médica Mundial. Declaración de Helsinki de la Asociación Médica Mundial. Principios éticos para las investigaciones médicas en seres humanos. Fortaleza: 64.ª Asamblea General de la AMM; 2013 [cited 2019 Apr 5]. Available from: <https://goo.gl/hvf711>.
21. **Coley B, Jolles BM, Farron A, Bourgeois A, Nussbaumer F, Pichonaz C, et al.** Outcome evaluation in shoulder surgery using 3D kinematics sensors. *Gait Posture.* 2007;25(4):523-32. <http://doi.org/cqm7km>.

22. **Van Hees VT, Gorzelniak L, Dean León EC, Eder M, Pias M, Taherian S, et al.** Separating Movement and gravity components in an acceleration signal and implications for the assessment of human daily physical activity. *PLoS One*. 2013;8(4):1-10. <http://doi.org/f2z3xs>.
23. **Cook KF, Roddey TS, Gartsman GM, Olson SL.** Development and psychometric evaluation of the Flexilevel Scale of Shoulder Function. *Med Care*. 2003;41(7):823-35.
24. World Health Organization (WHO). Obesity: preventing and managing the global epidemic. WHO; 2000 [cited 2017 Sep 7]. Available from: <https://bit.ly/2TXBxvj>.
25. **Sugamoto K, Harada T, Machida A, Inui H, Miyamoto T, Takeuchi E, et al.** Scapulohumeral rhythm: relationship between motion velocity and rhythm. *Clin Orthop Relat Res*. 2002;401:119-24. <http://doi.org/cwemcd>.
26. **Laursen B, Jensen BR, Sjøgaard G.** Effect of speed and precision demands on human shoulder muscle electromyography during a repetitive task. *Eur J Appl Physiol Occup Physiol*. 1998;78(6):544-8. <http://doi.org/c7mn7c>.
27. **Aviv AJ, Sapp B, Blaze M, Smith JM.** Practicality of accelerometer side channels on smartphones. In: Annual Computer Security Applications Conference. Orlando: ACSAC; 2012. 41-50.