Comparison of the flexural strength of sheets manufactured in three types of zirconium dioxide with two sintering times

Comparación de la resistencia flexural de láminas elaboradas en tres tipos de dióxido de zirconio con dos tiempos de sinterización

Edgar Torres¹, Elias George², Ismer Tami³, Jessika Gutierrez⁴

Oral Rehabilitator. Laboratory Coordinator, Fundación Universitaria CIEO - UniCIEO. ORCID: 0000-0002-1385-983X

Oral Rehabilitation Intern, Fundación Universitaria CIEO - UniCIEO. ORCID: 0000-0003-1463-8550

Oral Rehabilitation Intern, Fundación Universitaria CIEO - UniCIEO. ORCID: 0000-0003-4979-975X

Oral Rehabilitation Intern, Fundación Universitaria CIEO - UniCIEO. ORCID: 0000-0003-4443-6538

Abstract

Introduction: yttrium-stabilized zirconium dioxide (zirconia) has been used to manufacture fixed partial prosthesis due to its high flexural strength. However, there are no available studies comparing the effect of two sintering techniques on flexural strength. This study aims to compare the flexural strength of zirconia sheets manufactured with two sintering techniques. *Method:* for this in vitro study, three zirconia disks were used (Upcera: Super Translucent (ST): 1200 MPa, Multi-Layer (ML): 600 MPa and High Translucent (HT): 1200 MPa), using an Isomet[®] cutter to prepare 60 sheets 2 mm thick, 5 mm wide and 37 mm long. These sheets were randomly distributed into two groups of 30: the first group was sintered for 8 hours at 1,530°C and the second group was subjected to fast sintering for 3 hours at 1,530°C. The flexural strength in Newton was measured on an Instrom® 3366 Universal Testing Machine. The results were converted from N to MPa flexural strength, and compared by ANOVA and t test. Results: no statistically significant difference was found in the flexural strength of the two groups (p>0,05). Conclusion: the two compared sintering procedures do not affect the flexural strength of zirconia sheets.

Resumen

Introducción: las restauraciones de dióxido de zirconio estabilizadas con ytrio para prótesis parciales fijas e implantosoportadas se han utilizado por su alta resistencia flexional. En la revisión bibliográfica no se encontraron estudios que comparen la resistencia flexional del dióxido de zirconio con 2 tiempos de sinterización diferentes. El objetivo del presente estudio consistió en comparar la resistencia flexional de láminas elaboradas en 3 tipos de dióxido de zirconio con 2 tiempos de sinterización. Método: en este estudio in vitro, se recolectaron 3 discos de dióxido de zirconio (Upcera: Súper translúcido (ST): 1200 MPa, Multicapa (ML): 600 MPa y Alta translucidez (HT): 1200 MPa), y en un aparato de corte Isomet® se recortaron 60 láminas de 2 mm de espesor, ancho de 5 mm y longitud de 37 mm. Estas láminas se distribuyeron aleatoriamente en dos grupos de 30: el grupo uno se sinterizó por 8 horas a 1.530°C y el otro grupo se sometió a sinterización rápida por 3 horas a 1.530°C. La resistencia flexional se midió en una máquina universal Instrom® 3366. Los resultados fueron convertidos de N a MPa y se compararon mediante análisis de varianza y prueba t. Resultados: no hubo diferencia estadísticamente significativa al comparar la resistencia flexional después de dos tiempos de sinterización diferentes (p>0,05). Conclusiones: no se presentaron diferencias significativas en la resistencia flexional del dióxido de zirconio al comparar los promedios obtenidos con dos técnicas de tiempo de sinterización diferente.

Submitted: September 10/2019 - Accepted: October 06/2020





Keywords:

mechanical

properties, ZrO.

Palabras clave:

resistencia

propiedades mecánicas,

dióxido de

zirconio

flexional,

How to quote this article: Torres E, George E, Tami I, Gutierrez J. Comparison of the flexural strength of sheets manufactured in three types of zirconium dioxide with two sintering times. Rev Fac Odontol Univ Antioq. 2020; 32(2): 75-81. DOI: http://dx.doi.org/10.17533/udea.rfo.v32n2a7

INTRODUCTION

Fixed partial prostheses (FPP) are used to replace missing teeth. Historically, gold was considered the best prosthetic material, but in 1789 Martin H. Klaproth discovered zirconium, and in 1990 zirconium dioxide (zirconia) started to be used as filling material for composite resins, implant abutments, intra-radicular retainers, FPP substructures, and single crowns.¹

In nature, zirconium is a bright, malleable, grevish material. Its flexural strength is about 1,000 MPa, with a Young's modulus of 200 GPa, Vickers hardness of 200 MPa, and melting temperature of 1,855°C.² It is obtained as a zirconium powder that must be processed to eliminate impurities, mostly hafnium oxide (HFO₂) because it is very similar to zirconia and according to the 133-56 ISO Standard, only less than 5% is allowed. During this procedure, aluminum dioxide is added to improve mechanical properties and reduce hydrothermal degradation. The compaction process is done by one of two techniques at 1,000 kg x cm² the uniaxial pressing technique that consists of introducing zirconium powder in a mold to be compacted in only one direction, while in the isostatic pressing technique the material is compacted in various directions. Using the isostatic technique, the material's linear shrinkage is eliminated, but its cost is higher.³

The crystalline phases of zirconia are directly related to thermic changes. The monoclinic phases are found at room temperature or less than 1,170°C; the tetragonal phase is stable at 1,170°C-2,370°C, and the cubic phase is stable at temperatures over 2,370°C. Three generations of zirconia materials have been developed. The first generation is partially stabilized zirconia, which was

used 15 years ago for FPP substructures; it has a high refraction index that yields opacity, and its flexural strength is 1,000-1,200 MPa, indicated for single crowns, 4-unit FPP and free ends FPP. To improve optical properties, the second generation of zirconia was developed in 2012-2013, with the same strength and indications but with aluminum dioxide grains redistributed by the infiltration technique. To further improve optical properties, the third generation of fully stabilized zirconia was launched in 2015 with two mixed phases (tetragonal and cubic); it was more translucent and eliminated hydrothermal degradation. Its flexural strength is 550-650 MPa and is indicated for single crowns, veneers, inlays, onlays and anterior FPP. It is manipulated by 3D stratification or multilayer.⁴

Sintering is the final treatment of zirconium dioxide. Hummler defines this process as the transportation of a thermal mass that reinforces the particles among them and/or changes their porosity and geometry, coupled with free energy reduction.⁵ This process takes 8 hours in conventional ovens but this time is reduced to 3 hours in the latest generation ovens.

Stawarczyk et al⁶ determined the effect of sintering temperature on the flexural strength, contrast relationship and grain size of zirconia, using a three-point test of resistance. They concluded that the ideal range of sintering temperature is 1,500°C-1,550°C and that if temperature is increased over 1,700°C the mechanic properties are abruptly reduced, although esthetic properties are improved.

Jenni Hjerppe et al⁷ evaluated the effect of different surface treatments on the flexural strength of zirconia at a temperature of 1,500°C in a fast sintering oven (3 hours). They did not find statistically significant changes in mechanical properties.

Sedda et al⁸ used a Zircomat T[®] oven for 8 hours (conventional sintering) and did not find differences in the mechanical properties either.

Dahl et al⁹ used two sintering techniques and measured Vickers hardness and flexural strength but found no differences.

The goal of selecting a fast sintering technique is to reduce working time. Therefore, the objective of the present study was to compare the flexural strength of sheets manufactured in 3 kinds of zirconium dioxide using two sintering times, measured on a universal testing machine.

METHOD

The protocol of this study was evaluated by the Institutional Ethics Committee and approved as a study with no risk according to Resolution 8430 of 1993.

The calculated sample size was 9 sheets per subgroup, but to increase reliability, 10 sheets were used per subgroup, for a total of 60 sheets distributed into two groups: 30 for conventional sintering and 30 for fast sintering. Each group was distributed in 3 subgroups: 10 HT sheets; 10 ST translucent sheets and 10 ML sheets.

Three zirconium dioxide disks were prepared with Upcera[®], ST:1200 MPa, ML:600 MPa and HT:1200 MPa; using the Isomet[®] cutting device of the UniCIEO biomaterials laboratory, 60 sheets of 2 mm thick, 5 mm width x 37 mm length were prepared. Sheets were measured with a Mitutoyo[®] digital micrometer.

The sheets were dried in a Zirkonzahn[®] lamp for 1 hour and then subjected to sintering either in the Zircomat T[®] conventional oven for 8 hours at 1,530°C, or Zircomat 6000 MS[®] oven for 3 hours at 1,530°C, at the Eurodent Dental Academy in Bogotá.

Flexural strength was measured on an Instrom[®] 3366 universal testing machine, applying the three-point test, which consists of 2 fixed points to sustain the sheets and a central point to apply force. The results in Newton (N) were converted to MPa, using the formula indicated by the 6872: 2008 ISO standard:¹⁰ MPa = 3NI / 2bd², where MPa = Fracture strength in MegaPascal, N = Fracture load, I = distance between support points, b = width, and d = thickness.

The statistical analysis was performed using the Minitabs 18 software. Normality of distribution was tested by a graph, and comparisons were made by ANOVA and *t* test.

Table 1. Results of the ANOVA test for sintering groups

Source	DF	SC Adjust.	MC Adjust.	F Value	p Value
Time	1	35,369	35,369	0.28	0.601
Material	2	1,707,704	853,852	6.70	0.003
Oven material	2	45,746	22,873	0.18	0.836

Source: by the authors

RESULTS

Figure 1 shows that data distribution is normal, and therefore parametric tests are applicable.

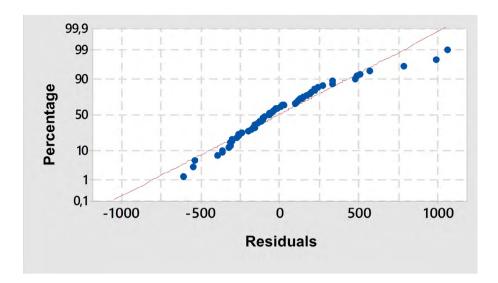


Figure 1. Graph of probability for normal distribution of the variables

Source: by the authors

The analysis of variance shows that flexural strength is not statistically different when sintering times are compared (p = 0.6 > 0.05). The difference between materials is significant (p = 0.003). The interaction of the two variables (oven x material) is not significant (p = 0.836).

The *t* test for ST material between ovens shows that the difference in flexural strength is not statistically significant (p > 0.05). Figure 2 shows that both averages are almost identical.

Figure 3 shows similar flexural strength averages in the two sintering groups.

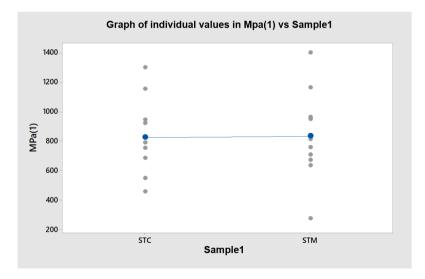


Figure 2. Graph of individual values for the two samples in MPa

Source: by the authors

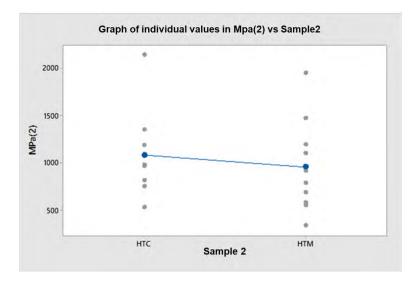


Figure 3. Graph of individual values for the two groups in MPa

Source: by the authors

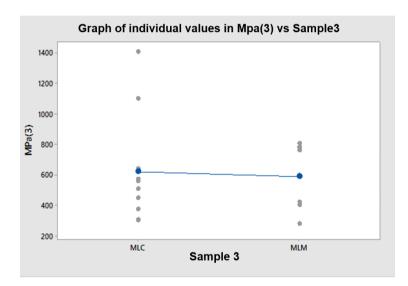


Figure 4. Graph of individual values for the two groups in MPa

Source: by the authors

The *t* test for the ML material between ovens shows no statistically significant difference (p > 0,05).

DISCUSSION

The results of the present study clearly show that there are no significant differences in flexural strength between the materials, regarding sintering procedures. However, the difference between materials is significant as expected because the selected materials had different properties.

Both averages are higher than the values reported by the manufacturer. This can be explained because the manufacturer does not indicate the test used, while the present study followed the 6872: 2008 ISO Standard.

Starwarcy et al⁶ studied the sintering techniques considering the hypothesis that the mechanical and optical properties could be altered by temperature changes occurring during the processing of zirconium dioxide. They found out that the best range of temperatures was 1,500°C-1,550°C, with no significant difference in mechanical properties after sintering, in agreement with the results of the present study.

Starwarcy et al¹¹ also studied the effect of sintering temperatures on the esthetic properties, concluding that the last generation zirconia is more translucid. This property is inversely proportional to the mechanical properties. Therefore, it is important to consider the esthetic requirements of each restoration. In the present study, the translucid property of zirconia was not assessed, but it is known that there is a direct correlation between optical properties and temperature.

Sedda et al⁸ studied the effect of shading processes on the flexural strength of zirconia blocks. They obtained results for flexural strength in pre-shaded zirconia blocks under neutral, slight, medium or intensive infiltration, finding out that there are no statistically significant differences in flexural strength in the presence of a fast sintering process. The reported values are similar to those obtained in the present study. In a study measuring density and other zirconium properties after two different sintering procedures (fast and conventional), Dahl et al⁹ found no difference in Vickers hardness or flexural strength, also agreeing with the present results.

It is recommended for future studies to compare the flexural strength of other kinds of zirconia and to compare the mechanical behavior of zirconia with different optical properties.

CONCLUSION

No significant differences in zirconium dioxide flexural strength were found when comparing the average values of two procedures with different sintering times.

CONFLICTS OF INTEREST

The authors declare that they have no conflicts of interest.

CORRESPONDING AUTHOR

Ismer Tami Fundación Universitaria CIEO - UniCIEO (+57) 3015429087 ismer_tami@hotmail.com Carrera 55 No. 152b-68 Mazuren 1, Apto 808, Torre 1 Bogotá, Colombia

REFERENCES

- 1. Hu L, Wang Ch. Effect of sintering temperature on compressive strength of porous yttrium-stabilized zirconia ceramic. Ceram Int. 2010; 36(5):1697-01. DOI: https://doi.org/10.1016/j.ceramint.2010.03.009
- 2. Montagna F, Barbesi M. Biomateriales dentales y procesos de laboratorio dental cerámicas, zirconio y CAD/CAM. En: Cerámicas, Zirconio y CAD/CAM.Venezuela: Amolca; 2013, p 151–78.
- 3. Ebeid K, Wille S, Hamdy A, Salah T, El-etreby A, Kern M. Effect of changes in sintering parameters on monolithic translucent zirconia. Acad Dent Mater. 2014; 30(12):419–24. DOI: https://doi.org/10.1016/j. dental.2014.09.003
- 4. Piconi C, Rimondini L, Cerroni L. El zirconio en odontología. Bogotá: Panamericana; 2011.
- 5. Acevedo A, Castañeda A, Milanes I. Comparación al MEB de diferentes tratamientos térmicos de y-tzp rectificados con fresas de diamante post-sinterización [Thesis]. Bogotá: UniCIEO; 2012.
- 6. Stawarczyk B, Ozcan M, Hallmann L, Ender A, Mehl A, Hmmerlet CHF. The effect of zirconia sintering temperature on flexural strength, grain size and contrast ratio. Clin Oral Investig. 2013; 17(1): 269-74. DOI: https://doi.org/10.1007/s00784-012-0692-6
- Hjerppe J, Narhi O, Pekka K, Lassila L. Surface roughness and the flexural and bend strength of zirconia after different surface treatments. J Prosthet Dent. 2016; 116(4): 577-83. DOI: https://doi.org/10.1016/j. prosdent.2016.02.018
- 8. Sedda M, Vichi A, Carrabba M, Capperucci A, Louca C, Ferrari M. Influence of coloring procedure on flexural strength of zirconia blocks. J Prosthet Dent. 2015; 114(1): 98-102. DOI: https://doi.org/10.1016/j. prosdent.2015.02.001
- 9. Dahl P, Kaus L, Zhao Z, Johnsson M, Nygren M, Wiik K et al. Densification and properties of zirconia prepared by three different sintering techniques. Ceram Int. 2007; 33(8); 1603-10. DOI: https://doi. org/10.1016/j.ceramint.2006.07.005
- Stawarczyk B, Keul C, Eichberger M, Figge D, Edelhoff D, Lümkeman N. Three generations of zirconia: from veneered to monolithic. Part II. J Quintessence Inter Rest Dent. 2017; 48(5): 369-80. DOI: https:// doi.org/10.3290/j.qi.a38057
- 11. Stawarczyk B, Keul C, Eichberger M, Figge D, Edelhoff D, Lümkemann N. Three generations of zirconia: from veneered to monolithic. Part I. J Quintessence Inter Rest Dent. 2017; 48(6): 441-50. DOI: https://doi.org/10.3290/j.qi.a38157